CLAIMS:

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1. Method for calculating a clogging factor of a filter composed of hollow-fiber membrane, which has a blood inflow portion and a blood outflow portion, for filtering a blood by passing said blood, said method comprising the steps of:

measuring at least two pressure selected from the group consisting of a pressure in said blood inflow portion, a pressure in said blood outflow portion, a filtering pressure in said blood inflow portion, and a filtering pressure in said blood outflow portion; and

calculating a filter clogging factor indicating the reduction in flowing ease of the blood in said filter and/or a filter clogging factor indicating the reduction in ease of filtering of said filter, by using the measured pressure.

- 2. Method for calculating a clogging factor of a filter according to claim 1, wherein a filter clogging factor indicating the reduction in flowing ease of the blood in said filter is calculated by using a viscosity of blood.
- 3. Method for calculating a clogging factor of a filter according to claim 1, wherein a filter clogging factor indicating the reduction in ease of filtering of said filter is calculated by using a viscosity of liquid waste.
- 4. Method for calculating a clogging factor of a filter according to claim 1, wherein a filter clogging factor indicating the reduction in flowing ease of the blood in said filter is calculated by using structure information and/or flow rate information of said filter.
- 5. Method for calculating a clogging factor of a filter according to claim 1, wherein a filter clogging factor indicating the reduction in ease of filtering of said filter is calculated by using structure information and/or flow rate information of said filter.
- 6. Method for calculating a clogging factor of a filter according to claim 2 or 4, wherein a filter clogging factor [F(%)], which the reduction in flowing ease of the blood in said filter is represented by the decreasing rate in a cross sectional area inside

said hollow-fiber, is calculated by using the Equation (1):

$$F=100\{1-[10^{-9} \cdot K \cdot 1 \cdot \eta_b \cdot (Q_b-Q_f/2)/N/\Delta P_b'/\pi]^{0.5}/R_0^2\}$$

Equation (1)

where K represents a correction coefficient (-), η_b represents viscosity(Pa·sec) of the blood, Q_b represents flow rate(ml/min) of the blood flowing into the filter, Q_f represents filtering flow rate (ml/min), N represents the number of hollow-fibers (-), ΔP_b ' represents a difference(mmHg) of the pressure between both ends of the hollow-fiber, 1 represents an effective length(m) of the hollow-fiber, and R_0 represents the radius (m) inside the hollow-fiber that the clogging does not occur.

7. Method for calculating a clogging factor of a filter according to claim 2 or 4, wherein a filter clogging factor [F(%)] which the reduction in flowing ease of the blood in said filter is represented by the decreasing rate in a cross sectional area inside said hollow-fiber is calculated by using the Equation (2):

$$F{=}100\{1{-}[K' \cdot \eta_b \cdot (Q_b{-}Q_f/2)/\Delta P_b]^{0.5}\} =$$

Equation (2)

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where K' represents a correction coefficient (-), η_b represents viscosity(Pa·sec) of the blood, Q_b represents flow rate(ml/min) of the blood flowing into the filter, Q_f represents filtering flow rate (ml/min), and ΔP_b ' represents a difference(mmHg) of the pressure between both ends of the hollow-fiber.

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- 8. Method for calculating a clogging factor of a filter according to claim 1, 2, 4,6 or 7, wherein, a filter clogging factor indicating the reduction in flowing ease of the blood in said filter is calculated in real-time.
- 30 9. Method for calculating a clogging factor of a filter according to claim 3 or 5, wherein a filter clogging factor [f(%)], which the reduction in ease of filtering of said filter is represented by the decreasing rate in a cross sectional area of pore of said hollow-fiber, is calculated by using the Equation (3):

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f=100[1-(10⁻⁹ · k ·
$$\tau$$
 · Δ X · η w · $Q_f/r_0^2/A_k/A_m/\Delta P_w$ ') 0.5]

Equation (3)

where k represents a correction coefficient (-), τ represents a rate of curved path, Δ X represents a thickness of a membrane, η_w represents a viscosity of liquid waste passing a filter(Pa·sec), Q_f represents filtering rate(ml/min), r_0 represents the radius (m) of a hollow-fiber membrane pore that the clogging does not occur, ΔP_w represents a difference of the pressure between the blood side end and the liquid waste side end in the membrane pore of the filter(mmHg), A_k represents a proportion of a cross sectional area of the membrane pore to a unit area of the membrane in the filter, and A_m represents an area(m²) of the membrane in the filter.

Method for calculating a clogging factor of a filter according to claim 3 or 5, wherein a filter clogging factor [f(%)], which the reduction in ease of filtering of said filter is represented by the decreasing rate in a cross sectional area of pore of said hollow-fiber, is calculated by using the Equation (4):

$$f=100[1-(k' \cdot \eta_w \cdot Q_f/\Delta P_w')^{0.5}]$$

Equation (4)

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where k' represents a correction coefficient (-), η_w represents a viscosity of liquid waste passing a filter(Pa·sec), Q_f represents filtering rate(ml/min), r represents the radius (m) of a hollow-fiber membrane pore that the clogging does not occur, and ΔP_w ' represents a difference of the pressure between the blood side end and the liquid waste side end in the membrane pore of the filter(mmHg).

- Method for calculating a clogging factor of a filter according to claim 1, 3, 5,9 or 10, wherein, a filter clogging factor indicating the reduction in ease of filtering of said filter is calculated in real-time.
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- Method for calculating a clogging factor of a filter according to claim 1,2,4 or 8, wherein a filter clogging factor [S(-)] which the reduction in flowing ease of the blood in said filter is represented by the decreasing rate in a cross sectional area inside said hollow-fiber is calculated by using the Equation (5):

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$$S{=}[~\eta_{b} \cdot (Q_{b}{-}Q_{f}/2) \cdot ~\Delta~P_{b0}{'}/~\eta_{b0}/(Q_{b0}{-}Q_{f0}/2)/~\Delta~P_{b}{'}]^{0.5}$$

Equation (5)

- wherein η_b represents viscosity(Pa·sec) of the blood flowing in the hollow-fiber, η_b represents viscosity(Pa·sec) of the priming liquid in the priming, Q_b represents flow rate(ml/min) of the blood flowing into the filter, Q_{b0} represents flow rate(ml/min) of the priming liquid flowing into the filter in the priming, Q_f represents filtering flow rate (ml/min), Q_{f0} represents filtering flow rate (ml/min) in the priming, ΔP_b represents a difference(mmHg) (Pa-Pv) of the pressure between both ends of the hollow-fiber, and ΔP_{b0} represents a difference(mmHg) of the pressure between both ends of the hollow-fiber in the priming.
- 13. Method for calculating a clogging factor of a filter according to claim 1,3,5 or 11, wherein a filter clogging factor [s(-)] which the reduction in ease of filtering of said filter is represented by the decreasing rate in a cross sectional area of membrane pore of said hollow-fiber is calculated by using the Equation (6):

s=
$$(\eta_w \cdot Q_f \cdot \Delta P_{w0}' / \eta_{w0}/Q_{f0}/\Delta P_w')^{0.5}$$

Equation (6)

wherein η_w represents viscosity(Pa · sec) of the liquid waste, η_{b0} represents viscosity(Pa · sec) of the liquid waste in the priming, Q_f represents filtering flow rate (ml/min), Q_{f0} represents filtering flow rate (ml/min) in the priming, ΔP_w represents a difference(mmHg) of the pressure between blood side end and liquid waste side end of the hollow-fiber membrane pore, ΔP_{w0} represents a difference(mmHg) of the pressure between blood side end and liquid waste side end of the hollow-fiber membrane pore in the priming, and s represents a ratio of cross sectional areas in the hollow-fiber membrane pore of the filter.

14. Method for calculating a clogging factor of a filter according to claim 1,3,5,11 or 13, wherein, an average of ΔP_w ' in said blood inflow portion and ΔP_w ' in said blood outflow portion is used as ΔP_w '.

- 15. Method for monitoring a clogging of a filter comprising the steps of:

 calculating a clogging factor of a filter by using a method for calculating a clogging factor of a filter according to any one of claim 1 to 14; and

 monitoring a clogging of a filter on the basis of the clogging factor of a filter.
- 16. Apparatus of monitoring a clogging of a filter comprising:

 means for calculating a clogging factor of a filter by using a method for calculating a clogging factor of a filter according to any one of claim 1 to 14; and means for monitoring a clogging of a filter on the basis of the clogging factor of a filter.
 - 17. Bed-side system comprising apparatus of monitoring a clogging of a filter according to claim 16.

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